



## Design and development of a Pupilometer for the automatic detection of Relative Afferent Pupillary Defect

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**ABSTRACT**—The presence of Relative Afferent Pupillary Defect (RAPD) indicates serious ocular disease, if untreated may lead to loss of vision. Swinging Flash Test (SFT) has been a traditional way of testing for RAPD for decades, quantification of RAPD, its reliability and accuracy is still not a reality. In this study, a novel Pupilometer device is proposed which uses custom-built hardware and software to perform the test to determine the RAPD at an early stage. The hardware of the device consists of components to produce a light stimulus into each eye and record the response of the pupils to the stimulus with a high-resolution camera. A Graphical User Interface (GUI) developed is responsible for the timing of the stimulus, processing the recorded response of the pupil in calculating the area of the pupil through image segmentation and analysis. RAPD test was conducted on 30 patients who are diagnosed with RAPD by using the pupilometer designed. The Pupil area of 30 RAPD patients has shown to be significant with  $p < 0.001$  in the diagnosis of RAPD.

**KEYWORDS**—RAPD, SFT, Constriction and Dilation, Light stimulus, Pupil Identification and Tracking, Pupillary Light Reflex.

### 1. INTRODUCTION

The eye is a complex, important, and special sense organ of the five sense organs of the human body. It helps us in viewing the world and plays a vital role in our day-to-day lives. Vision is a complex phenomenon of perceiving information about the environment in the form of reflection of light from objects that falls on the eye. The human visual system comprises various complex structures, each one performs a specific task, and they are interconnected to each other. The retina is the main functional unit of the eye that causes the transformation of light energy into action potentials and generates a neural signal, which is further transferred to the brain through the optic nerve. The optic nerve fibres are responsible for one of the important neurological reflexes called the light reflex, which refers to the constriction of both pupils when light is flashed into either eye, through afferent fibres called pupillary fibres, via the afferent nerve pathway. In a nervous system, the afferent pathway indicates the signal transmission from the sensory organ to the brain (from the eye to the midbrain). When the normal afferent pathway of the pupil is disturbed by any Ocular disorders the pupillary light reflex is affected leading to Relative Afferent Pupillary Defect (RAPD) [1,2]. The pupils respond briskly to stimulation of the good eye and weakly to stimulation of the diseased eye. Normal pupils, when light is projected into one eye, pupils of both eyes constrict equally and then relax a little. They dilate again when the light is removed. When the light is swung

rapidly between both pupils (within the meantime pupillary constriction), they maintain their state of constriction. When the time that the light present in front of each eye exceeds the mean pupillary constriction time of those pupils, they relax a little, equally when light is swung to both eyes. The characteristics within both eyes should be the same as a response to a stimulus.

The paradoxical dilation of both pupils when light is shone in front of a diseased eye is called RAPD. Since RAPD can be observed in anterior optic tract lesions, it provides a clue that how much afferent input must differ between the eyes to produce a clinically visible RAPD. The grading of RAPD is a useful indicator of the degree of damage that occurred in a diseased Optic Nerve. RAPD has a major role in determining the ocular health status [3,4]. Pupil Evaluation involves an examination of the size of the pupil, pupillary response, shape of the pupil and pupillary reflexes. Swinging Flashlight Test (SFT) is performed for Pupil Evaluation, where a flashlight is swung alternatively between both eyes and the pupillary responses are observed relative to each other. The difference between the pupillary reactions of the two eyes in RAPD patients is highlighted by the Swinging Flashlight Test. We will miss an RAPD if we do not perform SFT, as it is only by comparing the relative strengths of the signals reaching the brain that it is detected. Though the test is standardized over all these years, it is a subjective test, and the findings vary between observers. It requires a lot of learning, skills, and experience to perform SFT correctly and to interpret the results properly. All the characteristics of SFT should be met by every single practitioner to get correct and comparable results from everyone. Due to these limitations, the utility of the device for detecting RAPD must be tested on patients with known grades of RAPD and Normal subjects and comparing the results obtained between both groups [5].

Radzius, Aleksandras, et al. worked on an Infrared pupilometer that measures the pupil diameter and the change in pupil diameter after its response to a light stimulus and the values obtained were comparable to a photographic measurement [6]. Lada Kalaboukhova, Vanja Fridhammar, and Bertil Lindblom studied patients with Optic Atrophy due to Unilateral Open-angle glaucoma to develop a new technique to analyze RAPD and to find the optimum stimulus parameters for RAPD detection in those patients. They used a custom-built pupilometer and different sets of stimulus-pause combinations were studied (1s-0.5s, 0.5s-1s, 1s-1s, 1s-1.5s, and 1.5s-1.5s) and their study results showed that the combination of a stimulus duration of 0.5 s and a pause duration of 1 s at a light intensity of 1000 cd/m<sup>2</sup> was best suited for the detection of glaucoma [7]. The relative afferent pupillary defect was shown quantitatively in an eye contralateral to dense unilateral cataract, recorded using a binocular infrared video Pupillography. The difference between contraction amplitudes (which was defined as the difference between maximal and minimal diameters of the pupil of an eye) was larger when compared between right eye stimulation and left eye stimulation before the surgery with constrictions being higher when the cataractous eye was stimulated. This difference in contraction amplitude disappeared after surgery in the cataractous eye. Pupillary responses were examined quantitatively in three patients with unilateral extensive myelinated nerve fibres and amblyopia using a binocular infrared video pupillographic device (Vision module; Newopto, Kawasaki, Japan) in a darkened room by presenting stimuli with white light-emitting diodes to the right and left eyes alternatively. They noticed that there was per cent reduction in pupil contraction amplitude (the sum of both pupils) during the stimulation of the affected eye. The average of constriction amplitudes (constriction amplitude for each light reflex was defined as the

difference between maximum and minimum diameters) for the four right eye stimulations was then compared with the average of the four left eye stimulations.

Cohen, Liza M., et al., worked on a Novel and Computerized pupillometer. The pupil responses obtained in RAPD patients are correlated with the RAPD stimulated by presenting different illumination intensities (LUX) to both eyes and the clinician determined RAPD was correlated with the device-calculated RAPD. They found a significant correlation in both cases. They determined the eye with RAPD, and the degree of it is calculated with the ratio of percentage change in the constriction amplitude to the right eye and left eye under stimulation. Based on study results they concluded that the device had high sensitivity and specificity. As per the literature, this is the only available device which can detect the eye with RAPD and the degree of RAPD [8]. Volpe, Nicholas J., et al., say that the pupillometer device distinguishes between healthy volunteers and patients with RAPD greater than 0.9 log units of neutral density filter reducing its sensitivity. In this study, there is a significant statistical difference between normal and RAPD patients and a significant correlation between patients with true APDs and subjects with stimulated RAPD's using neutral density filters [9]. Cox, Terry A worked with a binocular television pupillometer and recorded the pupillary responses of normal subjects after stimulating RAPD using neutral density filters to dim the light in front of one eye while performing the swinging flashlight test. They aimed to determine the best indicator of RAPD by comparing contraction amplitude, minimum size, final size, and dilatation amplitude. Their study concluded that the contraction amplitude was the best indicator [10]. Volpe, Nicholas J et al., again worked on a computerized pupillometer device. They compared the Neutral Density Filter (NDF) strength required to neutralize the RAPD of the patient for whom the device also calculates the absolute inter-eye difference, and they found a significant correlation between both findings. But there is also an inter-eye difference found by the device in normal subjects, which questions the device's capability in distinguishing normal from abnormal [11]. A study carried out using a pupillometer to determine whether there is any difference in constriction amplitude between both eyes in 10 patients with various degrees of amblyopia showed that only a small proportion of amblyopes show the difference in constriction amplitude. Dara Lankaranian compared the sensitivity and specificity of detecting RAPD using the routine Swinging flashlight test method and Pupillography method on patients having glaucoma and concluded that Pupillography with a magnified view of pupils helps in better detection of RAPD [12]. A study, done by Benson, M. T., et al. showed a positive scope for the further development of the device using which the mean difference of pupillary responses between the right and left eye was calculated. They found a significant difference between the mean differences of normal subjects and patients with RAPD. The mean difference between the right and left eyes was 8.84 ms for normals and 78.6 for patients with RAPD [13]. Shwe-Tin calibrated pupillometer output with the neutral density filters of attenuation: 0.0, 0.3, 0.6, and 0.9 log units and tested it on healthy volunteers by stimulating RAPD with NDF of the same attenuation. The sensitivity and specificity of the device detecting stimulated RAPD with NDF were high. Thus, they gave future directions for using this device to detect RAPD in actual patients [14].

Although there have been multiple studies describing many pupillometers and their use in detecting RAPD throughout many decades, to date there is no pupillometer that got incorporated into clinical practice and achieved widespread use.

This could be because of the lack of availability of an established pupillometer that is accepted and believed by clinicians which can replace a traditional swinging light test performed by a well-

experienced doctor in detecting the RAPD. RAPDx designed by Konan Medical a US-based company, is the only pupillomotor device which determines pupil function and gives a quantitative score of RAPD. Therefore, we are proposing a Novel device to standardize this test using custom-designed hardware and a software routine. The initial prototype of the device was designed and used on RAPD patients as an alternative method for SFT.

## 2. METHODOLOGY

The main objective of the project is to design and develop a Pupilometer for the detection of RAPD from the pupillary response obtained under the external visual stimulus. The response of the pupils is recorded by a high-resolution camera, and the video file is processed by using an image processing algorithm. Hardware Components and Software tools used in developing custom-designed hardware and software for the device are given in different sections. Pupilometer can be used on children above 6 years of age to adults who need an examination of the pupil in the fields of Ophthalmology, Critical Care, Neurology and General Medicine. The idea behind the design is to keep the design robust, simple, safe, portable, tamper-proof, with minimal fixtures or fastening, lightweight and cost-efficient. The design avoids the problem of light escaping to the other eye when the stimulus is in front of the other eye and illuminates one eye at a time correctly. For better detection of RAPD, the intensity of the light stimulus is maintained constant (Right eye – 1330 LUX and Left eye – 1140 LUX) throughout all 5 pairs of stimuli to each person. Light stimulus is ON for 3 seconds in front of each eye. The gap between each stimulus in the same pair and in between different pairs is 0.5s.



**Figure 1:** Proposed design of Pupilometer

### 2.1. Hardware Assembly

The proposed design of the pupilometer is shown in the figure.1 The components of the proposed Novel Pupilometer device are as mentioned below

- Eight White LED's

- Four IR LEDs
- Camera's
- Arduino Nano
- PCB
- Ambrane P-1000 Star Power Bank 10400 mA

The device comprises eight visible LED's four in front of each eye. They emit monochromatic light occurring at a single wavelength. Four Infrared light emitting diodes (IR LED) are positioned two in front of each eye helping in viewing the pupil under darkness. The device comprises two cameras ELP series USB webcams, one in front of each eye records the pupil reactions to light stimulus. The main assembly of the proposed novel Pupilometer is centred on the PCB mount. The PCB, apart from holding the Arduino Nano board and acting as a mount for the Cameras, helps connect all the LEDs. Arduino is programmed to provide visual stimulus through LED and pupillary response is recorded by the high-resolution cameras. A binocular eyepiece surrounds the webcams so that the field of view of the camera and the line of sight of the eye is along a straight line.

## **2.2.Specifications of the Hardware**

Consistency of stimulus: The stimulus is constant throughout all the pairs of Stimulus

The intensity of stimulus: Right eye – 1330 LUX and Left eye – 1140 LUX

Number of Stimulus pairs – Five pairs of stimuli for each person

ON time and OFF time - ON time is 3 seconds in front of each eye, and the gap between each stimulus in the same pair and in between different pairs is 0.5s.

Number of access ports: Ease of accessing the device - 2 ports connecting the device and Laptop/Computer

Neglected Components:

Distant target: To check if the distant target is mandatory for the detection of RAPD, patients with known grades of RAPD were tested by giving a near stimulus and allowing them to accommodate and then checked RAPD. The patients not only showed RAPD but also the grading was the same when they were given distant and near targets. So, we neglected the distant target compulsion to check RAPD.

Scotoma-free stimulus: The reason for using scotoma free collimated stimulus source is to illuminate one eye at a time and avoid illuminating another eye, the scotoma-free collimated light source is also neglected in the device.

## **2.3. Data Collection**

This study is conducted in collaboration with the Neuro-Ophthalmology department at L V Prasad Eye Institute (LVPEI). The outpatient department in LVPEI has been screened for RAPD patients on a day-to-day basis. The Electronic Medical Record system at LVPEI facilitated the easy screening of patients for RAPD. Information Posters were used to get patients, to keep Optometrists and Ophthalmologists informed about the need of RAPD patients for the study.

In LVPEI, patients are initially seen and worked up by Optometrists. As part of routine workup, the Pupil examination by the Swinging Flashlight test is also performed by the Optometrists. Any abnormality present in the pupils is noted down. All the patients are seen by the doctors before dilating them. If RAPD is present, the Senior Ophthalmologist tests and confirm the presence and grade of RAPD by doing a Swinging Flashlight test before dilating them for further examination.

### **2.3.1.Data Collection Protocol:**

Study Design: Experimental Case-Control Study

Study Site: L V Prasad Eye Institute, Hyderabad

Sample Size: 60 participants

Study group: 30 patients with RAPD

Control group: 30 Normal volunteers

Inclusion Criteria:

Study group:

- All grades of RAPD
- No efferent pupillary defects
- No other pupil disorders (Anisocoria, Irregular pupil, displaced pupils)

Control group:

- No ocular or systemic disorders
- No h/o any ocular or systemic medication that alters pupil size
- No RAPD

Exclusion Criteria:

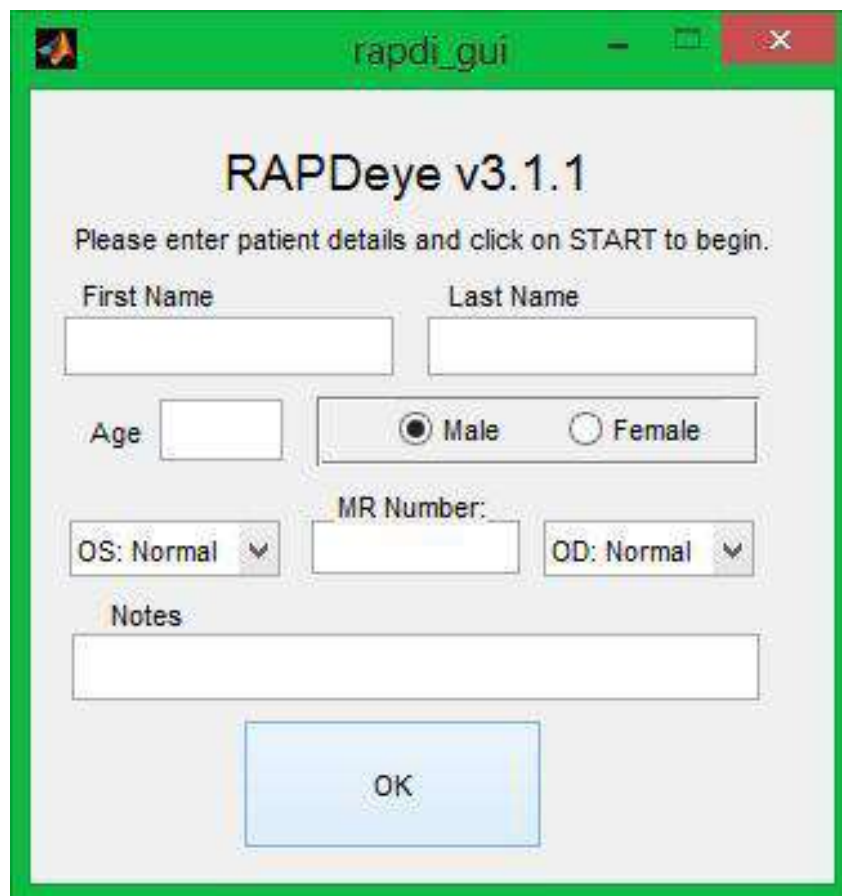
Subjects who are not falling under the inclusion criteria.



**Figure.2.** Experimental setup

Patients confirmed with RAPD and falling under the inclusion criteria were considered and explained briefly about the study before dilating them. If the patient agrees to take part in the study the patient along with their attendant were taken to the clinical setting room with the experimental

set-up shown in figure.2. The consent form is given, and the patient and the attendant were explained about the study in detail. They are allowed to read the consent and the signature is taken from the patient and the attended signature as witness. If the patients are not attended by anyone the signature of one of the team members is taken as witness.



**Figure.3.** Graphical User Interface of the Device

The patient details are entered into the RAPDeye Graphic User Interface shown in Figure.3. The GUI has a provision for creating the database consisting of personal information and patient history. Patients are asked to view from the window, and the device is adjusted so that the pupils of both eyes are visible correctly in the preview pane. The test starts by pressing the start button, stimulus alternates between both eyes by lasting in front of each eye for three seconds and a rapid alternation with a gap of 0.5 seconds between each stimulus pair. The cameras present inside the device record a live video of the pupil of each eye separately when they are reacting to light stimulus. Once the five stimulus pairs are completed the test will be stopped automatically. The video will get saved with the patients' MR Num. The total time taken for stimulus is 34.5 seconds and the whole procedure of explanation and taking signatures on the consent took less than 10 minutes.

The testing procedure is the same for the control group also except for the inclusion criteria which varied between them.

OpenCV, a computer vision and machine learning software library, is used to program the cameras to detect and track the pupil through the images of the recording. Both Arduino IDE and OpenCV have MATLAB interfaces. MATLAB code returns a video file saved with the patient's ID into the same storage device to which the pupilometer is connected. After the required number of stimulus pairs is given to the patient, the device is stopped manually. The video recordings obtained from the study group are processed and analyzed to observe the changes in pupil diameter concerning time. MATLAB program segregates the video file into multiple frames at a predefined rate. For each given frame, the area of the pupil, the state of light and the time interval of the frame are calculated. A graph is plotted with an area of pupil Vs time to get a pictorial and quantitative representation of the pupil responses. The proposed device was used in the control group of 30 normal volunteers and a study group of 30 RAPD patients as shown in table.1 to table.6.

**Table.1.** Number of Patients with RAPD

Gender	Number of patients
Males	13
Females	17

**Table.2.** No. of RAPD Patients with left and right

Eye with RAPD	Number of patients
Right	14
Left	16

**Table.3.** RAPD patients with different age groups

Age Range	Number of Patients
20-29	14
30-39	7
40-49	6
50-59	3

**Table.4.** RAPD grading of Left and right eyes

Grade	Right	Left
Grade 1	3	4
Grade 2	2	4
Grade 3	9	7
Grade 4	0	1



**Table.5.** Normal subjects' gender wise

Gender	Number of subjects
Males	3
Females	27

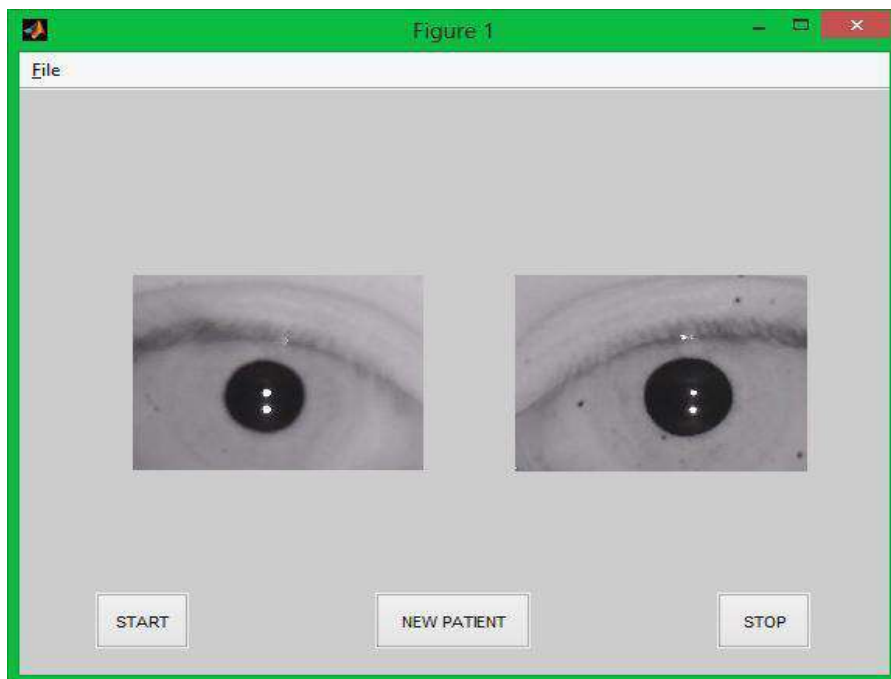
**Table.6.** Normal subjects with different age groups

Age range	Number of subjects
20-29	13
20-39	8
40-49	6
50-59	3

The experimental setup shown consists of the data collection pupilometer connected to a desktop/laptop with a Graphical User Interface (GUI) as shown in figure.4. Images acquired are pre-processed and the initial image is displayed in the preview pane as shown in figure.5.

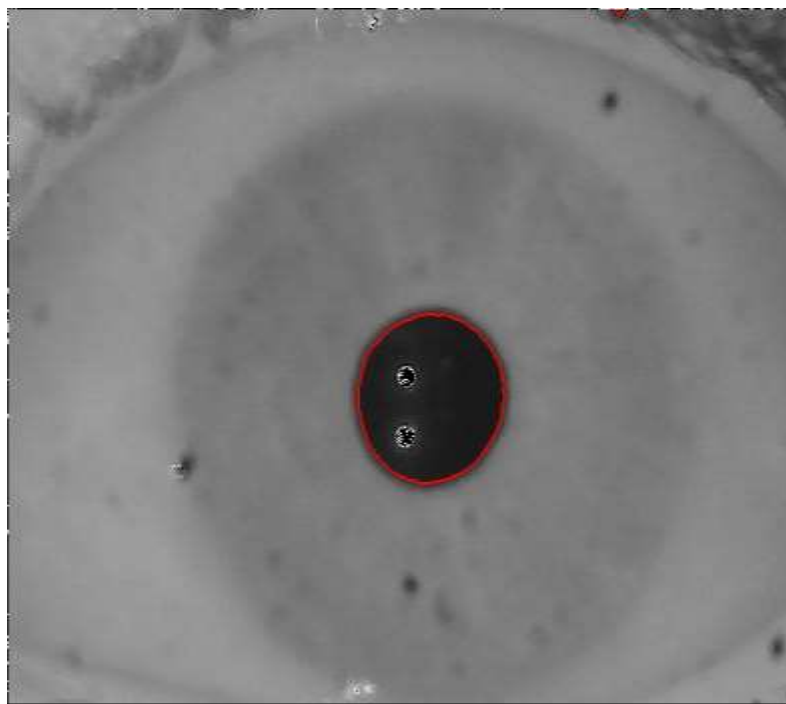


**Figure 4.** Data collection  
Stimulus Yellow – ON in front of the right eye  
Green – ON in front of the left eye

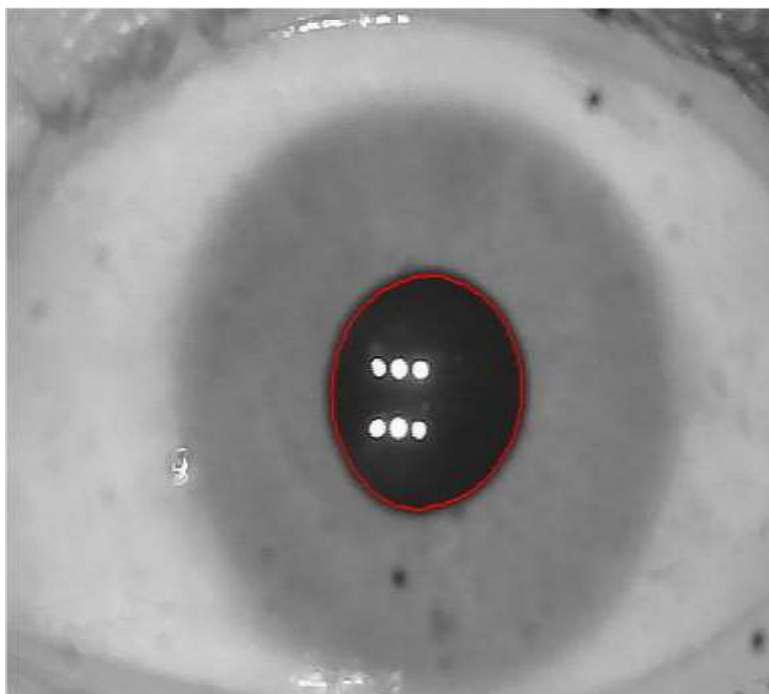


**Figure.5.** Preview of both eyes before starting the recording

Every video is divided into many frames. Each frame is processed using OpenCV libraries to detect pupils. The OpenCV software enables live detection and tracking of pupils in each frame followed by radius calculation of the same. The area of the pupil is calculated for all the frames in Pixels as shown in figure.6.

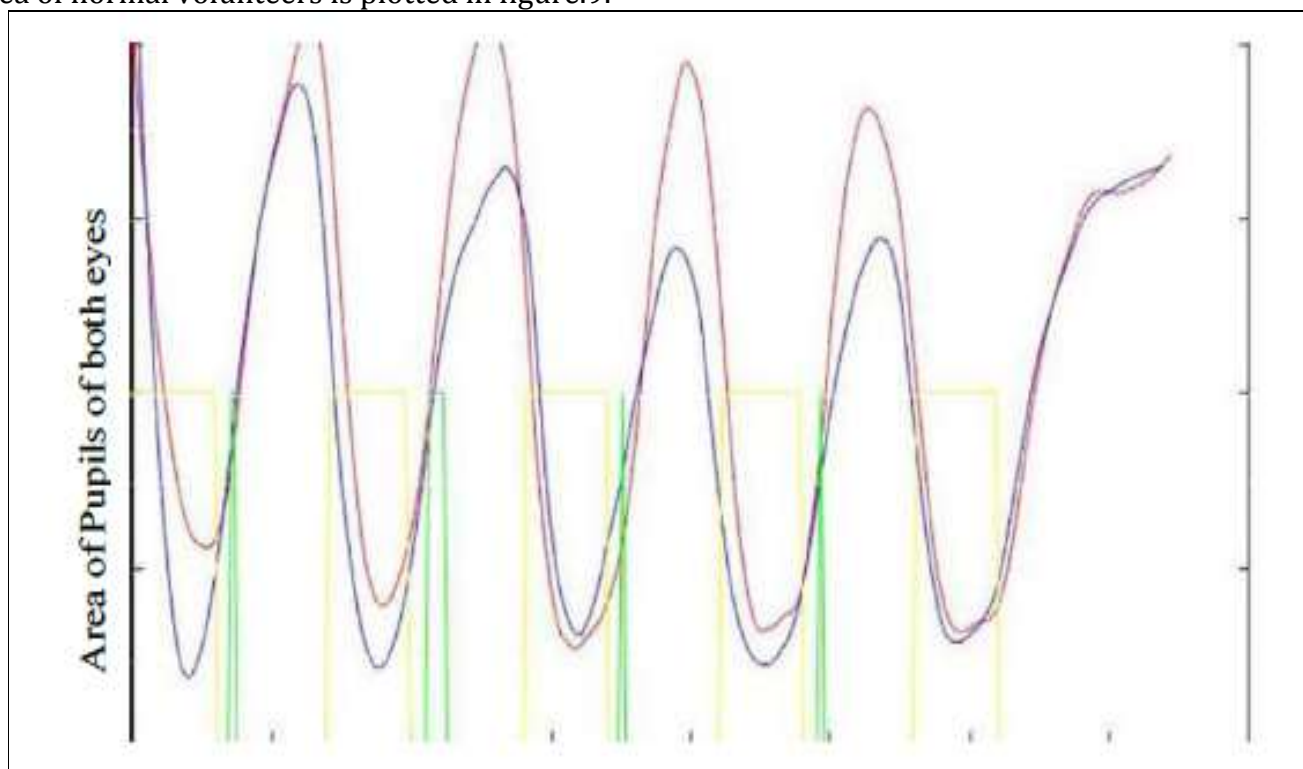


**Figure.6.** Segmented pupil of the eye under normal



**Figure.7.** Segmented pupil under Light stimulus

The pupil area of RAPD patients under the visual stimulus of both eyes is plotted in figure.8 in which the left eye is under the stimulation of yellow LED, right eye is with Green LED. Similarly, the pupil area of normal volunteers is plotted in figure.9.



**Figure.8.** Pupil area of RAPD patient

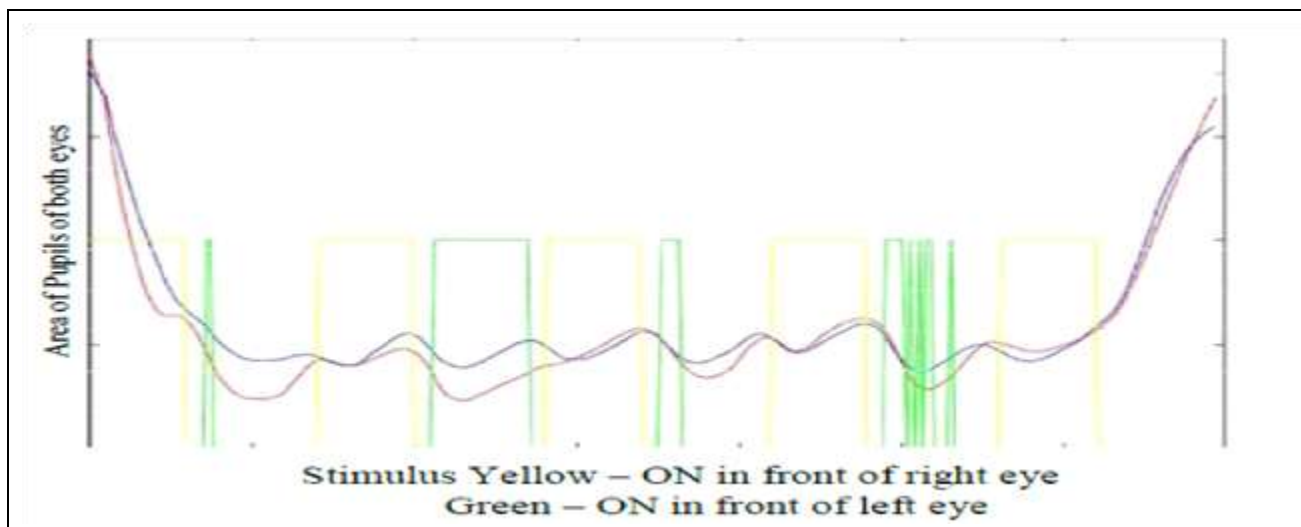


Figure.9. Pupil area of normal volunteer

### 3. RESULTS AND DISCUSSIONS

The difference between the "Mean ranks" score of the area of the pupil when "Stimulus ON in Right eye" Vs "Stimulus ON in Left eye" are checked in both the "Normal group" (figure 10 & 11) and "RAPD group" (figure 12 & 13). The Asymptomatic Significance (2-tailed) value indicates if the difference is significant between the two independent values "Stimulus ON in Right eye" and "Stimulus On in Left eye" about the dependent variable "Area of pupil". The difference between the "Sum of ranks" score of the area of the pupil when "Stimulus ON in Right eye" Vs "Stimulus ON in Left eye" can also be checked in both the "RAPD group" and "Normal Group".

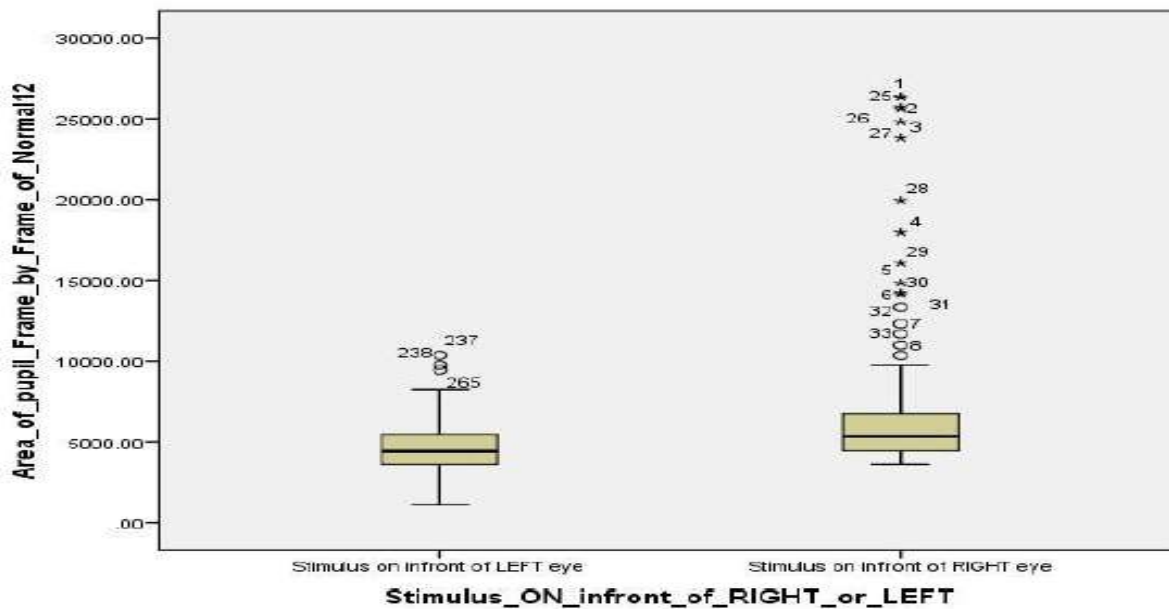
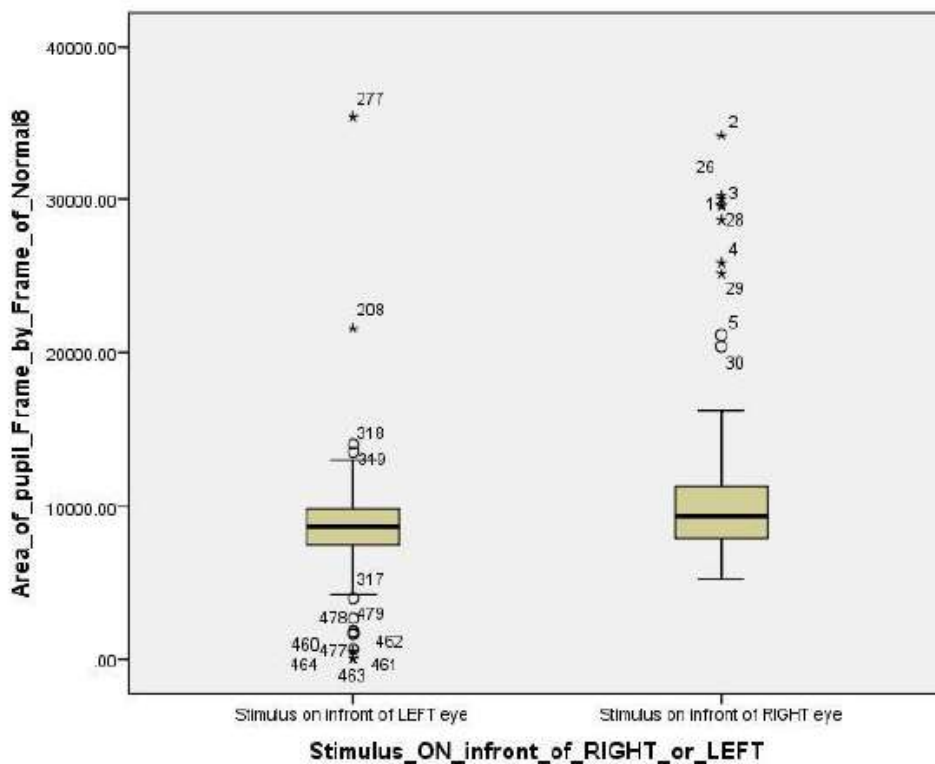
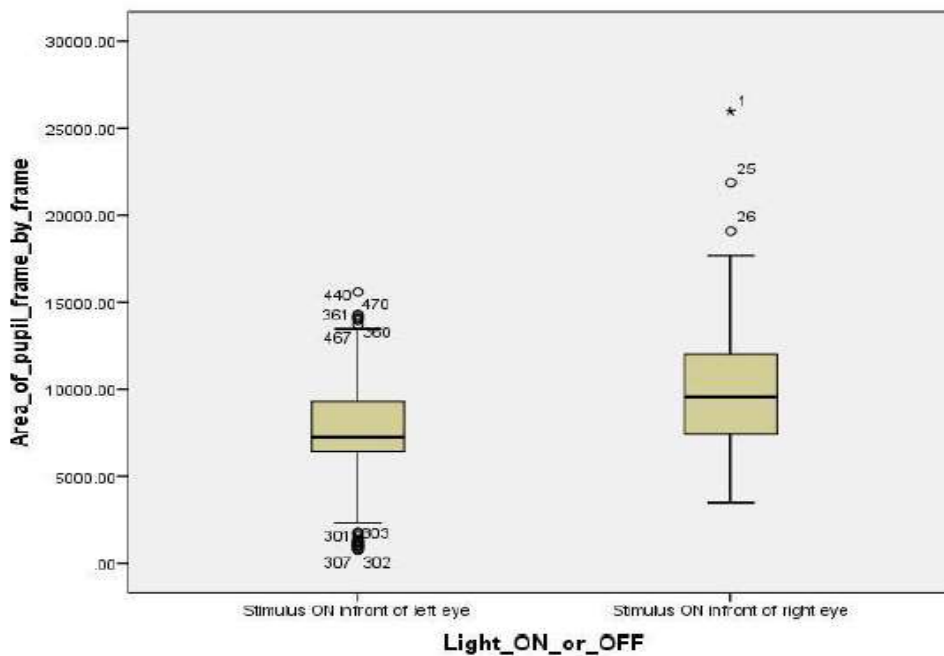


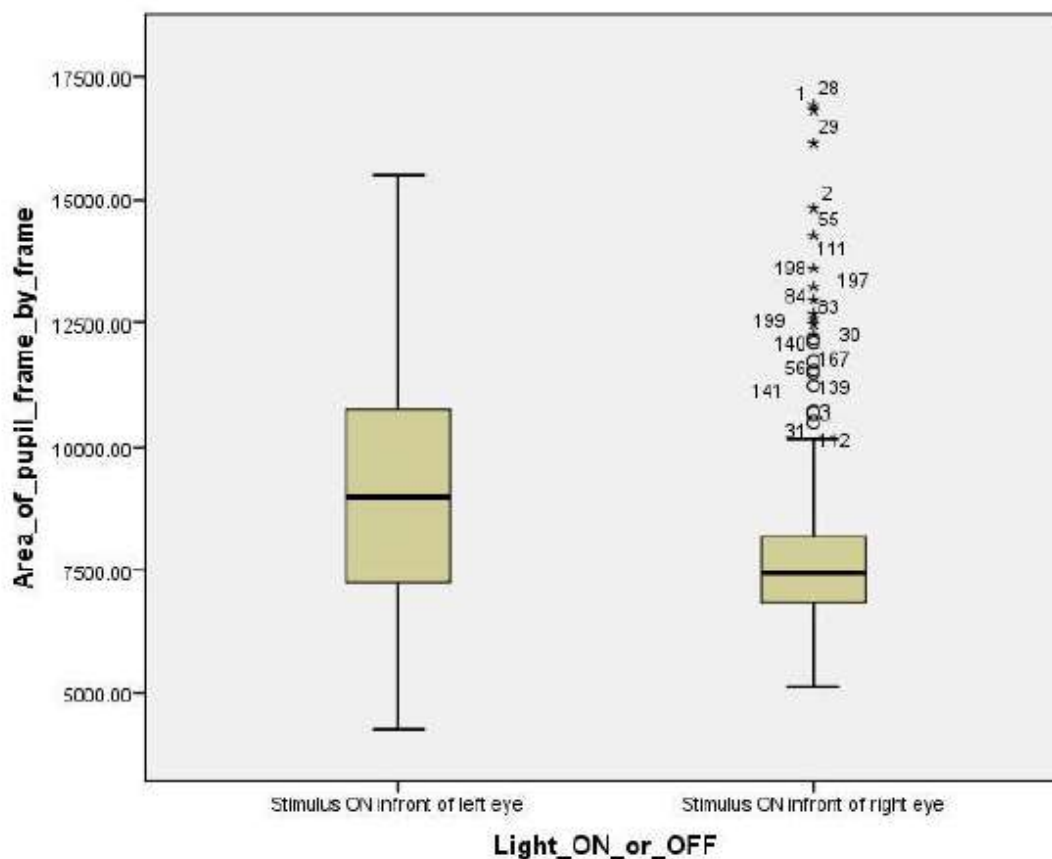
Figure.10. Area of pupil frame by frame of normal12



**Figure.11.** Area of pupil frame by frame of normal8



**Figure.12.** Area of pupil frame by frame of RAPD5 patient



**Figure.13.** Area of pupil frame by frame of RAPD8 patient

### 3.1.RAPD Group

In the RAPD group, all the results clearly show that the Mean rank and Sum of the rank of area are high in the "Eye with RAPD" when the stimulus is ON in that eye compared to the good eye (Un affected eye) in all patients except three. The Asymptomatic Significance (2-tailed) score shows that the difference in Mean ranks when Stimulus is ON in the RAPD eye Vs Stimulus ON in the Good eye is highly significant in all the patients. In Patient 13 (grade 3), Patient 19 (grade 1), and Patient 24 (grade 1) the Mean ranks are high in the good eye rather than the RAPD eye and the Significance of the difference between these two groups is also high.

### 3.2.Normal Group

When Stimulus ON in the Right the Mean ranks are high in 22 Normal volunteers and when Stimulus ON in the Left Mean ranks are high in 8 Normal volunteers. The difference is always present between the two variables "Stimulus ON in Right" Vs "Stimulus ON in Left". The difference is significant in 21 Normal volunteers and not significant in the rest 9 Normal volunteers. Out of 21 significant Normal volunteers, when the Stimulus is ON on the Right the Mean rank is high in 16 Normal and for the rest 5 Normal the Mean rank is high when the Stimulus is ON on the left. Out of 9 significant Normal volunteers, the Mean rank is high in 6 Normal's when Stimulus is ON on the Right and 3 Normals when Stimulus is ON on the Left. The reasons for the presence of significant area difference when

Stimulus ON in Right” Vs “Stimulus ON in Left” in Normal’s also could be due to the limitations present which are still being worked on. In patients with RAPD, due to damage in the pupillary pathway, the pupils are eye larger by default. When light falls on the eye with RAPD, as the pupils dilate naturally, most of the time the LED flashes are within the pupil and the area is calculated correctly. When light falls on the good eye the pupils constrict naturally and the area of the pupil which is already smaller is calculated much lesser. In Normal subjects, because there is no damage at all the pupils are normal and when light falls on either of them both pupils constrict very small. This leads to LED flashes falling on pupil borders and the area is calculated improperly.

**No repeatability:** As we cannot make sure that each time when the same patient is tested the pupils of positioned exactly at the same place in a frame, the area calculated for the same patient is completely different every single time.

**No relativity:** As we cannot say that in a relative or same frame of both eyes, the LED flash reflections are always within the pupil or outside the pupil similarly for both eyes, we cannot compare both eyes relatively. This could be the cause for the high difference in areas in Normal subjects.

### **3.3.Statistical Analysis**

Statistical Analysis Using the Mann-Whitney U test, a non-parametric test is performed to calculate the difference between obtained areas of the pupil in Right Vs Left eye stimulation. As the distribution of two groups (area values when the stimulus is on the Right and Left) have a different shape, mean ranks are compared rather than medians. In the RAPD study group, the results clearly show that the Mean rank and Sum of the rank of area are high in the "Eye with RAPD" when the stimulus is ON compared to the Un affected eye in nearly 80% of the patients.

### **4. CONCLUSIONS AND FUTURE SCOPE**

The proposed Novel device christened Pupil+ helps diagnose the ocular disease called, RAPD. At the current stage, the device met its objective of removing the human element in testing RAPD and differentiating between a Normal and RAPD patient only if the light stimulus falls within the pupil area of the eyes. The proposed project offers a wide scope of further improvements. The quality of the device can be improved in every aspect so that fully automated equipment which produces a complete report of pupil evaluation with several parameters can be developed at the industrial level for public use.

### **5. ACKNOWLEDGEMENTS**

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### **6. REFERENCES**

1. Clinical Anatomy of the Eye; Second Edition – Richard S. Snell, Michael A. Lemp
2. Clinical Anatomy of the Visual System; Second Edition – LEE ANN REMINGTON  
Jack J Kanski Clinical Ophthalmology; Sixth Edition

3. Bell, Raymond A., et al. "Clinical grading of relative afferent pupillary defects." *Archives of Ophthalmology* 111.7 (1993): 938-942
4. <http://www.richmondeye.com/clinical-content-the-relative-afferent-pupillary-defect>  
Radzius, Aleksandras, et al. "A portable pupilometer system for measuring the pupillary size and light reflex." *Behaviour Research Methods, Instruments, & Computers* 21.6 (1989): 611-618
5. Kalaboukhova L, Fridhammar V, Lindblom B. Relative afferent pupillary defect in glaucoma: a pupillometric study. *Acta Ophthalmol Scand.* 2007 Aug;85(5):519-25. doi: 10.1111/j.1600-0420.2006.00863.x. Epub 2007 Jun 15. PMID: 17573859.
6. Cohen, Liza M., et al. "A novel computerized portable pupillometer detects and quantifies relative afferent pupillary defects." *Current eye research* 40.11 (2015): 1120-1127
7. Volpe, Nicholas J., et al. "Portable pupillography of the swinging flashlight test to detect afferent pupillary defects." *Ophthalmology* 107.10 (2000): 1913-1921 1005-14-740117
8. Cox, Terry A. "Pupillographic characteristics of simulated relative afferent pupillary defects." *Investigative ophthalmology & visual science* 30.6 (1989): 1127-1131
9. Volpe, Nicholas J., et al. "Computerized binocular pupillography of the swinging flashlight test detects afferent pupillary defects." *Current eye research* 34.7 (2009): 606-613
10. Enyedi, Laura B., Sundeep Dev, and Terry A. Cox. "A comparison of the Marcus Gunn and alternating light tests for afferent pupillary defects." *Ophthalmology* 105.5 (1998): 871-873.
11. Graefe, A.; Mitteilungen vermischten Inhalts: 12: Ueber ein einfaches Mittel, Simulation einseitiger Amaurose zu entdecken, nebst Bemerkungen ueber die Pupillar-Kontraktion b<sup>^</sup>i Erblindeten. *Arch. f. Ophth.* 2:266 (pt. 1) 1855.
12. Gerold, Hugo. *Die Lehre vom schwarzen Staar u. dessen Heilung.* Rubach, 1846
13. Hirschberg, J. "Neuritis retrobulbaris." *Z. Prak. Augenh* 8 (1884): 185.
14. Baquis, E. "La reazione pupillare come elemento diagnostico differenziale tra l'amaurosi isterica e quella da nevrite retro-bulbare." *Ann. Ottal* 30.3 (1901): i901
15. Gunn, R. Marcus, et al. "Discussion on retro-ocular neuritis." *The British Medical Journal* (1904): 1285-1287.
16. Kestenbaum, Alfred. *Clinical methods of neuro-ophthalmologic examination.* Elsevier, 2013.
17. LEVATIN, PAUL. "Pupillary escape in disease of the retina or optic nerve." *AMA Archives of Ophthalmology* 62.5 (1959): 768-779
18. Thompson, H. Stanley. "Afferent pupillary defects: Pupillary findings associated with defects of the afferent arm of the pupillary light reflex arc." *American Journal of Ophthalmology* 62.5 (1966): 860-873 1005-14-74011755
19. Thompson, H. St. "Pupillary signs in the diagnosis of optic nerve disease." *Transactions of the ophthalmological societies of the United Kingdom* 96.3 (1976): 377