



Investigating Drug Release Kinetics from Biocompatible Guar Gum (GG)/Methyl Cellulose (MC) Blend - γ -Fe₂O₃ Nanocomposites

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ABSTRACT

This research explores the use of water-soluble biocompatible polymers, guar gum (GG) and methyl cellulose (MC), alongside the nanomaterial maghemite (γ -Fe₂O₃), for transdermal sustained drug release, employing metoprolol succinate as a model drug. Drug-infused thin film patches of GG, MC, their γ -Fe₂O₃ nanocomposites, and 10/90 GG/MC blend - γ -Fe₂O₃ nanocomposites were utilized for the investigation. Physicochemical parameter evaluations, including thickness, weight, folding endurance, % moisture absorbance, and % moisture loss, supported the drug release kinetics study using a hydrated cellophane sheet and diffusion tube. The results indicate that this blend-nanocomposite system releases the drug through diffusion, following Fickian kinetics. These biomaterials hold promise for developing slow, sustained release formulations in transdermal drug delivery systems.

Keywords: blend-nanocomposites, guar gum, methyl cellulose, maghemite, compatibility, biocompatibility.

1. INTRODUCTION:

Researchers are increasingly focused on developing novel drugs and dosage forms to enhance efficacy while reducing side effects. Water-soluble polymers are being extensively utilized in the pharmaceutical industry [1-7]. The irregular shifts in drug concentration in the bloodstream resulting from conventional dosing have prompted the development of

controlled drug delivery systems [8, 9]. Transdermal drug release systems (TDRS) capitalize on the skin for drug administration, utilizing biocompatible polymer patches for improved absorption, patient compliance, bioavailability, and easy termination [10].

The biocompatible polymers guar gum [11-15] and methyl cellulose [16, 17], and the nanomaterial maghemite (γ -Fe₂O₃) have been commonly used in sustained drug release (DRS) applications [18, 19]. The bulging behavior of guar gum and the ability to hold water and gel forming characteristics of methyl cellulose has contributed to controlled drug release and the patches have shown promise in providing sustained drug release profiles [20, 21]. Metoprolol succinate serves as a model drug in this research, known for its solubility, cardiovascular applications, and sustained release formulations [22].

In our previous work we have found that maghemite nanoparticles acts as a compatibilizer the 10/90 GG/MC blend composition [23]. This research work is aimed at studying the transdermal sustained drug release kinetics from the GG/MC blend – γ -Fe₂O₃ nanocomposite thin films using metoprolol succinate as the sample drug.

2. EXPERIMENTAL PROCEDURE:

In this study, Metoprolol succinate drug solutions were prepared, incorporating guar gum (GG), methyl cellulose (MC), their respective γ -Fe₂O₃ nanocomposites, and a 10/90 GG/MC blend - γ -Fe₂O₃ nanocomposite. Each solution, 50 mL in volume, was dispensed into uniformly sized polypropylene petri dishes. Subsequently, thin films were created within a dust-free environment, with each 1 cm² patch containing approximately 39.339 μ g of the drug. After drying, the films were carefully peeled from the substrate and subjected to analysis.

The thickness, weight, and other physicochemical parameters were measured with three identical samples and the average is taken. The percentage moisture absorption and moisture loss were calculated as per the procedure and using an appropriate formula [24].

The drug release studies were done using Systronics-2202 model spectrometer and open diffusion tube method. The Higuchi [25] and Korsmeyer-Peppas models [26] were applied to the release kinetics data to analyze the underlying drug release mechanisms, with n values indicating Fickian or anomalous diffusion, and $n \geq 1$ signifying zero-order release [26, 27].

3. RESULTS AND DISCUSSIONS:

3.1. Physicochemical evaluations

Table 1 presents the physicochemical evaluation data for metoprolol-infused GG, MC, their γ -Fe₂O₃ nanocomposites, and 10/90 GG/MC blend - γ -Fe₂O₃ films. The thickness ranged from 0.087 to 0.092 mm, with a nearly consistent weight of 218 to 223 mg. Folding endurance spanned 308 to 360, indicating robust strength. Methylcellulose exhibited higher folding endurance than natural guar gum, while maghemite nanoparticles slightly reduced it. These values affirm the usability of these patches for TDRS applications.

Table 1: Physicochemical parameters

Composition	Thickness (mm)	Weight (mg)	FE	PMA	PML
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GG	0.089 ± 0.0024	221.000 ± 1.549	314 ± 2	7.72 ± 0.80	3.16 ± 0.03
MC	0.087 ± 0.0012	218.167 ± 1.169	360 ± 2	4.56 ± 0.44	1.38 ± 0.00
GG – γ -Fe ₂ O ₃ composite	0.092 ± 0.0021	223.000 ± 1.095	308 ± 2	6.60 ± 0.28	2.38 ± 0.25
MC – γ -Fe ₂ O ₃ composite	0.091 ± 0.0018	222.167 ± 0.753	316 ± 2	4.51 ± 0.46	1.50 ± 0.26
10/90 GG/MC blend – γ -Fe ₂ O ₃ composite	0.087 ± 0.0018	218.000 ± 0.632	315 ± 1	5.19 ± 0.25	2.14 ± 0.27

To evaluate the structural durability of the thin films under both humid and dry conditions, standard protocols were followed to determine the percentage of moisture absorption and moisture loss. Remarkably, the inclusion of maghemite nanoparticles demonstrated an enhancement in both moisture absorption and moisture loss capacities within the thin films. Specifically, the analyzed samples displayed a moisture absorption percentage spanning from 4.51 to 7.72, accompanied by a moisture loss percentage ranging from 1.50 to 3.16.

3.2. TDRS kinetics

Figure 1 illustrates the drug release profiles from the thin films composed of GG, MC, their corresponding maghemite nanocomposites, and the 10/90 GG/MC blend - maghemite nanocomposites. Through the diffusion analysis, it was evident that the release of the drug from methylcellulose occurred rapidly as compared to guar gum. Notably, the maghemite nanocomposites formed with both methylcellulose and guar gum exhibited a sustained release pattern, contrasting with the immediate release of their pristine polymers. Furthermore, the drug release profile of metoprolol succinate from the 10/90 GG/MC blend - maghemite nanocomposite also demonstrated sustained behavior.

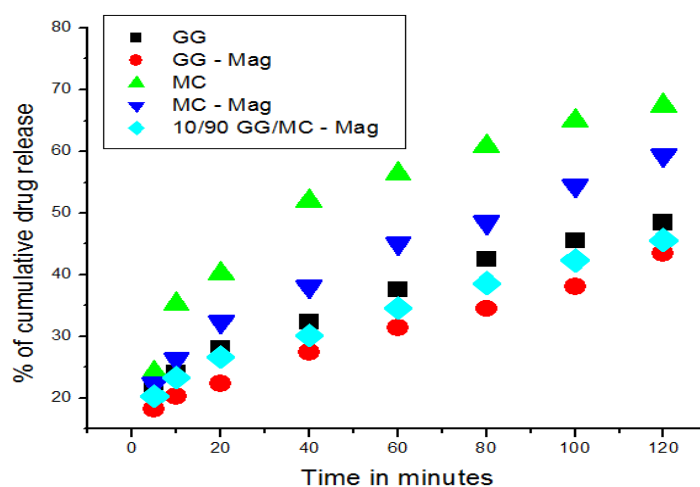


Fig. 1: Drug release kinetic data

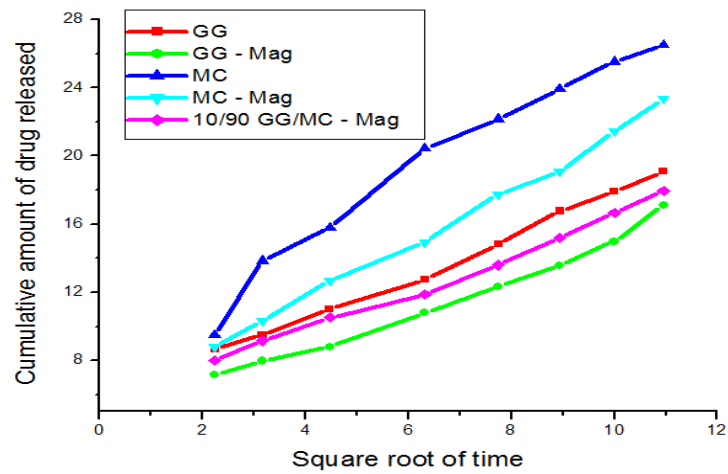


Fig. 2: Higuchi kinetics plot

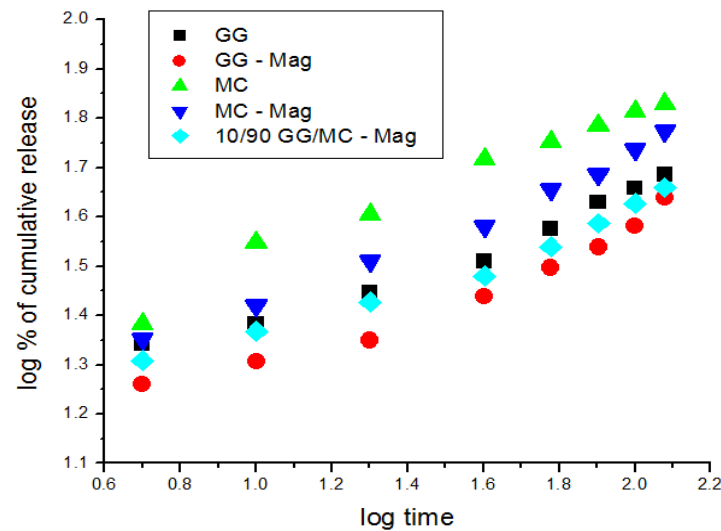


Fig. 3: Koresmeyer-Peppas kinetics plot

Table 2: The values from Koresmeyer-Peppas plot

Composition	Koresmeyer-Peppas model	
	Intercept (k)	Diffusion exponent (n)
GG	1.13636	0.25421
GG – $\gamma\text{-Fe}_2\text{O}_3$ composite	1.04097	0.2655
MC	1.20336	0.30718
MC – $\gamma\text{-Fe}_2\text{O}_3$ composite	1.12308	0.30138

10/90 GG/MC blend – γ -Fe ₂ O ₃ composite	1.1159	0.248
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The examination of drug release against the square root of time, utilizing the Higuchi method, serves to discern the release nature. A linear plot indicates diffusion control of the system [26]. Notably, the cumulative drug release versus square root of time plot (depicted in Figure 2) demonstrated linearity across all systems, affirming diffusion as the dominant release mechanism.

Subsequently, the experimental data obtained from in vitro release studies were fitted to the Korsmeyer-Peppas model. The resulting plot (illustrated in Figure 3) facilitated the determination of diffusion exponent "n" and constant "k," as outlined in Table 2. In all instances, the value of intercept "k" exceeded 0.5, while "n" was less than 0.5. These findings collectively support the conclusion that the drug release adhered to Fickian kinetics [26, 27]. As a result, these biomaterials hold potential for the formulation of controlled-release transdermal systems, offering slow and sustained drug release capabilities.

4. CONCLUSION:

This research investigated the potential of biocompatible polymers, guar gum and methyl cellulose, along with maghemite nanocomposites, for transdermal sustained drug release applications. Physicochemical evaluations showcased the suitability of these materials for patch formulation, with thickness, weight, and folding endurance values within desired ranges. The incorporation of maghemite nanoparticles showed improvements in moisture absorption and loss properties of the thin films. The transdermal drug release kinetics demonstrated distinct profiles, with methyl cellulose releasing the drug rapidly, while guar gum and maghemite nanocomposites exhibited sustained release behavior. The data fitting using Higuchi's and Korsmeyer-Peppas models confirmed diffusion-controlled release, indicative of Fickian kinetics. These findings underscore the potential of these biomaterials for developing effective and controlled transdermal drug delivery systems.

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