



A SURVEY ON MEDICAL IMAGE DATABASE WITH DEEP LEARNING P.Subshini¹

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Abstract

The medical industry has seen a surge in the use of artificial intelligence and machine learning techniques in recent years. Deep learning, the most current development in artificial intelligence technology, has allowed robots to mimic human intelligence in ever-more-complex and self-governing ways. Medical artificial intelligence systems used to primarily rely on experts to instruct computers by translating clinical data into logic rules specific to certain clinical scenarios. More advanced machine learning algorithms pick and balance relevant data to educate themselves to comprehend these principles by using data attributes, such as pixels from medical images or raw data from electronic health records (EHRs). Sorting through a medical image database turned out to be a little difficult. A support vector machine and cable neural network combination can be used to classify brain tumours from non-tumors in the input magnetic resonance pictures. This method of analysis was valued by the fig share dataset, which underwent analysis to produce a high degree of perfection. Properties of a cable neural network drove a multiclass support vector machine.

Keywords: Deep learning; Image database; Artificial intelligence; brain tumors.

1. Introduction

A significant advancement in the modern period was the disease known as CAD [1]. CAD is made feasible by an imaging technique, the development of learning concepts, an instrument for improved image processing, and an AML theory. Well-known subjects in medical image analysis and processing research include illness types, disease detection, and medical image retrieval dependencies [2]. Using medical photos, a technique to identify various diseases and their types was adopted, using distinct feature and algorithm classification extractions. An examination of a challenging tash revealed the proper mix of classifier and feature. Heuristics are utilised in this combo.

CNN is partially incorporated into a deep learning architecture. Convolutional neural networks are designed to function as a single, integrated unit that includes a classifier and an interest in the CAD system's operation. Convolutional neural networks are used in this work to classify breast cancer types as benign or malignant based on histological features. This work was expanded to include more

problems. In one study, tissue behaviour is assessed and described as a type of lung diagnosis. This

publication provides a study of the results and hyperparameter [3]. An association with the process of the art state bestows respect upon the architect. There are a variety of challenges encountered while modelling and implementing convolutional neural networks in the CAD process.

By classifying cells inside and outside the human brain in an infinite manner, an uncommon cell was generated. These cells unquestionably impair the brain's robust and proper processes. This kind of brain tumour can cause disabilities in the patient and occasionally even death. (6). There are two categories of brain tumours: benign and malignant. The benign tumour does not grow quickly outside of the body, and it is unaffected by the brain's robust structures. A malignant tumour has the potential to kill a person directly. In poor health, it will expand and readily impact other brain tissues. MRI scanning was one of the key scanning techniques. It was suggested that brain tumours in humans should be detected early on in order to prevent death. One unique technique to detect tumours was magnetic resonance imaging. When compared to CT scanning, it is thought to be an ideal scanning method. Using MRI technology, crucial information regarding the location, dimensions, form, and metabolism of the tumour was discovered. Procedures for identifying tissue errors are provided by this approach. It is an extremely powerful device that can detect both benign and malignant brain tumours.[7-10]

This study looks at a tumour classification method using magnetic resonance imaging data. Objective is defined as a three-part classification problem for differentiating brain characteristics. There are three types of brain tumours: meningioma, glioma, and pituitary [11]. These are the three most common types. For image extraction, a deep convolutional neural network was constructed and used with various SVM. Evaluation purposes were considered based on fig share. The medical professionals' therapy should be backed by a perfect CAD for the three tumours. And the second-high perfection group succeeds in the present difficult challenge that uses robust classifiers and deep learning approach.

2.Related work

A fundamental tumour with low effectiveness, often referred to as low rank in the patient's body, is gliomas. It may have a two-year lifespan and is also referred to as high rank. Molecular resonance Everyone has access to deep scans and recommended exams from imaga, which are used to detect brain tumours. A portion of the brain tumour helps us to organise medical interventions and determine the rate of development.

(Havaei, 2017) It has been demonstrated that magnetic resonance imaging is a potent technique that does not propagate illness and provides three-dimensional function assessment, analysis,tissue processing, metabolism,physiology, and imaging. See Prasad (2006). The output of a magnetic resonance image expands our understanding of the structure and components of an organism for medical study. Certain tumours, such meningiomas, are easily segmented, while glioblastomas are difficult to localise. Glioblastomas and gliomas are examples of tumours that divide images because

they are often diffuse and highly complicated. Texture in subareas can be altered by numerous experts.[13]

(Subbanna, 2013; Bauer,2011 and Hao,2012) The appearance of tissue, which was challenging to inspect during the tumor's generating process, and the tumor's shape or signal were monitored in order to analyse and distinguish it from normal brain structure in the case of the proposed brain tumour at the right side of the cerebrum [14]. Following the three-dimensional magnetic resonance imaging on a measured template from a normal brain, these anatomically-based operations took place. A conventional magnetic resonance imaging reproductive design is shown in the report. obtaining different levels of information, such as high- or low-quality magnetic resonance imaging, which is part of the clinical image preparation process.

3.Proposed scheme

A division that looks into this uses a cable neural network to separate the properties of magnetic support vector machines and brain magnetic resonance imaging. A comprehensive model of the inspected process was demonstrated. Processing: The size of the magnetic resonance imaging (265X265) was changed. Its grey values were standardised to fall between 0 and 1. A practical used cross-validation with the five-fold approach. The 3067 photos in the data set are matched to the group of 245 patients. Five roughly sized subsets were created from a single information set. the number of patients with an equal number of tumour divisions involved.In [16] Figure 1 depicted the pre-processing stages. In the provided diagram, indicators five and one represent the five disconnections of subsets that arose during the organisation of the five folded sections during cross-validation. In each validation step, one subset was assigned as a test and another as training. Following the five stages of validation, the model analyses and divides each magnetic resonance image.



Figure 1. experiment's dataset

Table 1 Hype-parameter settings of the experiment

Hyper parameter	CNN-SVM	CNN-Softmax
Optimizer	Adam	Adam
Mini-batch size	128	128
Loss	Hinge	Cross-entropy
L2 regularization factor	0.0001	0.0001
Kernel	Linear	-
initial learning rate	0.001	0.001
Epochs	20	20
Coding	Oise-ys-all	.
Classifier model	SVM-ECOC	Softmax

3.1 Architecture of Cable Neural Network:

A analysed division procedure extracts the features from a magnetic resonance picture using a cable neural network. 265X265 was one of the input segments of the investigated CNN design. There are two fully joined segments and five convolutional layers in a cable neural network configuration. These can be seen in Figure 3. In the cable neural network architecture, the convolution weight was connected to the entire joint form of the parameters. The design employed a variety of filters to capture different activations for the same image (input value). The borders of the image were safeguarded by assigning a pixel thickness of one. Different kernel sizes are chosen at different segments to capture the representation at different resolutions.

$$X_2 = \frac{X_1 - F + 2P}{s} + 1 \quad (1)$$

$$Y_2 = \frac{Y_1 - F + 2P}{s} + 1 \quad (2)$$

A layer's dimensions come after the terms listed below. The thickness of the input dimension was (X1,Y1,Z1), and the output size was (X2,Y2,K) after it was connected to the filter K and the size of (F,F). Measured as, X2 and Y2 are

3.2 Difficulty of cable neural network:

The values in the model of the investigated cable neural network include the computational challenges and memory requirements. The cable neural network's two segments were restricted by the model's consideration, and convolutional small filtering was prohibited. In a study of cable neural network design, the computations are accounted for by the level of convolution and dense junctions of fc segments. Multiplication and addition within layers were two functions of convolution. The quantity of addition and multiplication operations carried out in a convolutional layer according to dimension filters such as K, F2, and F1. Z, X, and Y were the features of the output dimension.

$$\text{Ops}_{\text{conv}} = F_1 * F_2 * K * X * Y * Z$$

The number of addition and multiplication processes in the FC layer matched the criteria. The addition of the number of mac processes made up the full mac process for the entire network.

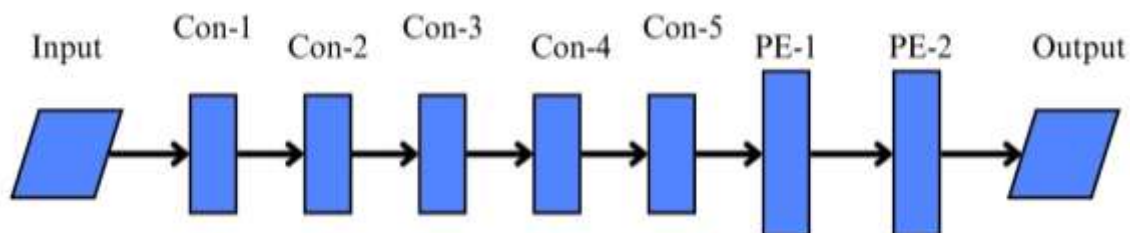


Figure 2. the full cable neural network layer and the convolutional segment

3.3 Cable Neural Network Memory requirements:

The amount of memory required to run the cable neural network design according to the specifications. The convolution layer and the FC layer both looked for the proper weight. Formula 4 was used to calculate the number of parameters for a convolution layer (Paramconv), where z stands for the number of input layers.

$$\text{Param}_{\text{conv}} = F_1 * F_2 * K * Z + K \quad (4)$$

The number of parameters for the FC layer (Param_{FC}) is calculated as,

$$\text{Param}_{\text{FC}} = X_{\text{erov}} * Y_{\text{erov}} = Z_{\text{Zurev}} * N_{\text{FC}} + N_{\text{FC}} \quad (5)$$

where X_{2n} , Y_{2ne} and Z_{man} represent the dimension of the layer previous to FC layer. Nic represents the number of output nodes for the FC layer. The computational overhead and the memory requirements determine the training time and test time required for a CNN.

4. Classification

The class labels are used to handle the numerous SVM designs, and the characteristics are separated from the images. To train SVM, the features extracted from the images are displayed. The outcome of the SVM design is the judged labels for the attributes. To assess the classifier performance, the evaluated labels were linked with the appropriate class. Three binary classifiers and a three division ECOC architecture are used in the work. Every binary process appeals to a linear one. Following the linear process experiment, the linear process was attached. The linear was assessed to yield accurate outcomes. The SVM algorithm and the ECOC model were obtained using the loss process.

4.1 Image Classification using M-SVM

The classifier receives the selected features in order to classify the magnetic resonance picture as abnormal. The two class complexes may be exploited by the binary SVM. These varieties involved the use of the Multiple Class SVM Division method, which is a variety of binary SVM classifiers. In a magnetic resonance picture, six classes of information were classified using a series of hybrid planes. To characterise the border from training data for an image, vectors may be used as input information components [23]. The joint that holds the characteristics of the input images was used to analyse the vector features. Throughout the experiment, the class may be examined by the classifier, and it was measured as

$$b = \operatorname{argmax}_{b'} \bar{w}^T \phi(\bar{a}, b) \quad (6)$$

Consequently, the formulation of the quadratic programme is provided as. The accurate and adjacent class constituted the margin. It was given the quadratic equation.

$$\forall_i \forall_b \neq b_i \bar{w}^T \phi(\bar{a}_i, b_i) - \bar{w}^T \phi(\bar{a}_i, b) \geq 1 - \epsilon_i \quad (7)$$

This kind of process was used to provide different divisions in different forms. The magnetic support vector machine separated the magnetic resonance imaging into two categories: abnormal image and correct picture.

5. EXPERIMENTAL SET- UP

On a computational process with 8 GB Random Access Memory and an Intel Xeon Central Processing Unit E3-1675-v6@4.90GHz, an experiment was successfully set up. This particular programme, Mathematicallab 2020, was utilised for the experiment. A sample image dataset.

On the information set from fig share, a categorization of tumour into pituitary, meningioma, and glioma was examined. It was an open data set that was mostly utilised for research-related difficulties as well as MIR and MIC issues (Cheng et al. 2015, 2016). A set of 3765 T-one CE was called an information set. 243 patients had parts engaged in magnetic resonance imaging. Meningioma, glioma, and pituitary tumours are among the three other tumours that are traced to two-dimensional sections. The information set was uneven and included 879 and 980 images of pituitary and meningioma tumours in addition to 1345 magnetic resonance images of gliomas. It measured 567 by 567. Table 2 displays the dataset's details.

Table 2. Details of Figshare dataset

Tumor Type	No.of Images	No.of Patients
Glioma	1426	89
Meningioma	708	82
Pituitary	930	62

Information corresponding to the five folds in cross validation was shared by several of the analyzers used in the multiple class division by fig. Following the validation trial, very few researchers observed division perfection. Every single image sample in the information set is looked at throughout the investigation phase once the cross validation was completed. Cross validation was used in the evaluation process, and it was shown to be a dependable method.

A study by Ismael and Abdel-Qader (2018) looked at the relationship between DWT and gabor features and NN depend division, finding a perfect division of 97.8%. The relationship between cable neural network properties and the ELM method is used for division in Pashaei et al. (2018)'s completed work. The cable neural network architecture consists of 4 segments and 349 filters with a size of (2X2). A kernel classifier is the foundation for the extreme learning approach used by some experts. Tab. 2 displays the fig sharing information set.

5.1 Evaluation by Harvard and Radiopaedia

For the specific three tumours under analysis in this work, Fig share served as a crucial source of information. It enables the examined division's investigative procedure to use the other set of information. Figures 3 and 4 depicted the relationship between the approaches under examination and the state of the art. It was separated into radio pedia set and Harvard. High perfection was achieved by an investigated approach using a cable neural network and soft max, achieving 97.5% and 99.1% for radio pedia and 98.5% and 98.1% for the Harvard set.

Table 3, Comparisca with state-of-the-art method for brain tumor detection using Radiopaedia dataset

Work	Accuracy (%)	Features	Classifier
Proposed	97.4	CNN	Softmax
Proposed	98.1	CNN	M-SVM
Molasen H. ef.al	96.5	CNN	CNN

Table 4. Comparison with state- of - be -art method for 4-class brain tumor classification using Harvard dataset

Work	Accuracy (%)	classifier	Features
Proposed	98.2	Softmax	CNN
Proposed	98.8	M-SVM	CNN
Mzoughi H.et.al	97.5	CNN	DWT

5.2 Examined process:

A minimum of two hours and six minutes were required for one complete trial of the five-fold approach during the cable neural network's training phase. As a result, the analysis was completed in less than a second at the minimum. This section discusses the division procedure, which was compared and evaluated using the art state method.

5.3 Correlated with other works:

Perfect division, which gives the percentage of accurate analysis produced by the division, was a crucial performance criterion for the division. Of them, a few are

- An ideal cable neural network design was employed as a DLC; - An ideal cable neural network design was combined with support vector machines.
- - An ideal cable neural network that works with a support vector machine.

Figure 4 displayed the validation and training progress. The success layer of a cable neural network classifier has a restriction. The features of support vector machines and cable neural networks were used to address it. In order to attain high perfection correlated to the given activation from convolution five layer, the process was therefore dependent on the properties of the cable neural network in the activation form from fc 1 layer.

5.4 Dividing image with DL method:

The deep learning technique CNN is used to effectively segregate the tumour from the brain MRI picture based on the kernels with less error rate and less time if the M_SVM classifier identified the MRI image as abnormal. CNN and M-SVM classifier are merged in this procedure.

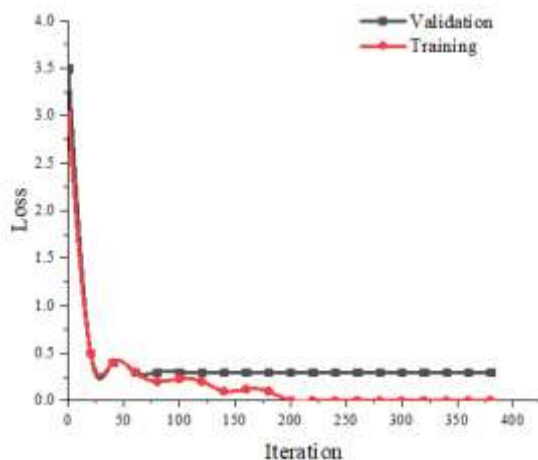


Figure 3. Losses in training and validation

The tumour can be segmented using a kernel-based CNN, and the tumour can be classified as benign or malignant using an M-SVM classifier. CNNs can have a broad formation and be multilayer neural networks. Currently, the widely used RBF (Radial Basis Function) kernel is used to choose the fundamental kernel intelligently. To increase flexibility for the tumour segmentation process, spectrum mixing is added to the basic kernel in this research. The kernel-based CNN is computed using the following equation (8).

$$K_{\text{CWN}} = \sum_{i=1}^l a_i \exp\left(1 - \frac{1}{2} \|\Sigma_i^{1/2}(q - q')\|^2\right) \cos(q - q', 2\pi\mu_i) \quad (8)$$

In this study, two distinct training stages were used to train the neural network to support two DLP layers for the tumour layer in magnetic resonance imaging. The first stage was used for the cable neural network's convol layer, while the second step was for the whole layer of the CNN model. During the learning process, the convolution cable neural network density was imitated. The linked segments are fully educated from the magnetic resonance image to the separate invisible layer in the second level of deep learning transmission. As a result, the tumour was identified using the kernel depend cable neural network from the magnetic resonance image.

5.5 Comparative Analysis:

CNN had to demonstrate that it could analyse brain imaging data more effectively than key traditional attributes. As a result, it was determined that the CNN classifier was more important than the softmax depend classifier.

5.6 Factors influencing the improved performance of M-SVM, CNN, and DL

Classifier

A layer of soft max is present in cable neural network architecture. A stand with a classifier is developed by a cable neural network with a layer of soft max. The phenomenon affected the process of the cable neural network. When there was a limited quantity of training data available, an effective overfitting was examined.

Softmax

The soft max mechanism was activated by the cable neural network. The method was described as

$$\sum_{j=1}^N$$

where the group of n variables is indicated by x. After the soft max process, the outcome is calculated as a possibility. The definition of cross entropy was

$$L_c = -\sum q_i \log(q_i)$$

where measures and facts for the result class were appraised by q and q'. When the true and judged values are near, a loss results in a low value. The proximity in the evaluations and judgements is calculated by a loss in entropy, which was investigated for gradient and more accurate computations. Penalties for wrong answers in MSE. MSE was not appropriate for an interpretation that could have been made using numerical data.

5.7 Improved function with Support Vector Machine:

A CNN softmax classifier uses probability to classify data and computes the outcome. One of CNN's drawbacks was overfitting. While a loss in validation does not result in zero, a loss in training does. Figure 4 made this very evident. The features indicate that overfitting was introduced into the CNN design. Information is classified using M-SVM by being converted to a high-dimensional value. This was the maximum optimisation contingent on hinge loss. The magnetic support vector machine's average margin model was poor.

The tab 5 and 6 displayed the results of the experimental analysis.

Table 5 Comparison with a transfer learning-based approach for brain tumor classification, evaluated using Figshare

Method	No. of parameters	Accuracy (%)	No. of layers	MAC operations
CNN with M-SVM	67M	99.2	8	0.78G
CNN (Softmax)	145M	98.9	17	14.8G

Table, 6 Summary of the experiments

Classification Problem	MRI dataset	Accuracy of CNN(softmax)(%)	Accuracy of CNN with M-SVM (%)
Brain tumor detection	Radiopaedia	97.4	98.1
4- calss brain tumor classification	Harvard	98.2	98.8
3-class brain tumor classification	Figshare	98.9	99.2

6 Conclusion:

To preserve human life, brain tumours needed to be identified and classified. These two presented difficult problems in the medical image analysis. It is thought to be significant for CAD. It develops as a result of the brain's uncontrollably increasing cell count. It was divided into two groups. They are both malignant and benign tumours. This study examines the operation of a cable neural network-based autonomous monitoring system using softmax and several support vector machine classes. It was made abundantly evident that the right learning processes provide flawless outcomes. Early brain tumour detection is undoubtedly helpful in keeping the patient safe. It helps the doctor handle patients correctly and gives them the motivation they need to get the best care possible. Classifying a medical image database proved to be somewhat challenging. Combining a cable neural network with a support vector machine allows for the classification of brain tumours and non-tumors in the input magnetic resonance images.

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